Accurate Multimodality Registration of medical images

M.V.Sruthi\textsuperscript{1}, Dr.K.Soundararajan, Dr.V.Usha Sree
\textsuperscript{1}Jawaharlal Nehru technological university Anantapur

Abstract—This paper presents a method of motion correction in registering multimodal imagery. Image registration is a vital problem in medical imaging. It has many potential applications in clinical diagnosis. It is a process of aligning two images into a common coordinate system. Thus aligning them in order to monitor subtle changes between the two. Registration algorithms will compute transformations to set correspondence between the two images. The purpose of this paper is to provide a comprehensive review of the existing literature available on Image registration methods in different modalities. It has been extensively shown that metrics based on the evaluation of mutual information are well suited for overcoming the difficulties of multi-modality registration. For this we are implementing multimodality registration algorithm which goals the motion correction.

Keywords—modality, interpolator, optimizer image registration

I. INTRODUCTION

Some of the most challenging cases of image registration arise when images of different modalities are involved. In such cases, metrics based on direct comparison of gray levels are not applicable. Image processing methods, which are possibly able to visualize objects inside the human body, are of special interest. Advances in computer science have led to reliable and efficient image processing methods useful in medical diagnosis, treatment planning and medical research. In clinical diagnosis using medical images, integration of useful data obtained from separate images is often desired. The images need to be geometrically aligned for better observation. This procedure of mapping points from one image to corresponding points in another image is called Image Registration. It is a spatial transform. In order to associate the information from modality, corresponding data in each image must be successfully registered. In long range surveillance applications the alignment function will register all objects in the scene. The reference and the referred image could be different because were taken

- At different times
- Using different devices like MRI, CT, PET, SPECT etc (multi modal).
- From different angles in order to have 2D or 3D perspective (multi temporal).

Image registration finds its applications in various fields remote sensing(multispectral classification), environmental monitoring, change detection, image mosaicing, weather forecasting, creating super-resolution images, integrating information into geographic information systems (GIS), in medicine (combining data from different modalities e.g. computer tomography (CT) and magnetic resonance imaging (MRI), to treatment verification, comparison of the patient’s data with anatomical atlases ,in cartography (map updating) and in computer vision (target localization, automatic quality control).

The concept of Mutual Information is derived from Information Theory and its application to One way to simplify the computation of the mutual information is to normalize the statistical distribution of the two input images. Image registration has been proposed in different forms by different groups.

II. IMPLEMENTATION

The metric requires a number of parameters to be selected, including the standard deviation of the Gaussian kernel for the fixed image density estimate, the standard deviation of the kernel for the moving image density and the number of samples use to compute the densities and entropy values. We should now define the number of spatial samples to be considered in the metric computation. Image registration is the process of determining the spatial transform that maps points from one image to homologous points on a object in the second image.

\begin{figure}[h]
\centering
\includegraphics[width=0.5\textwidth]{registration_diagram.png}
\caption{Diagram illustrating the concept of Image Registration.}
\end{figure}
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The basic components of the registration framework and their interconnections are shown in Figure 1. The basic input data to the registration process are two images: one is defined as the fixed image \( f(X) \) and the other as the moving image \( m(X) \). Where \( X \) represents a position in N-dimensional space. Registration is treated as an optimization problem with the goal of finding the spatial mapping that will bring the moving image into alignment with the fixed image. The transform component \( T(X) \) represents the spatial mapping of points from the fixed image space to points in the moving image space. The interpolator is used to evaluate moving image intensities at non-grid positions. The metric component \( S(f \circ m \circ T) \) provides a measure of how well the fixed image is matched by the transformed moving image. This measure forms the quantitative criterion to be optimized by the optimizer over the search space defined by the parameters of the transform.

Figure 2: MRI (fixed image) and a proton density MRI (moving image) are provided as input to the registration method.

The normalization filters are instantiated using the fixed and moving image types as input and the internal image type as output. The output of the readers becomes the input to the normalization filters. The output of the normalization filters is connected as input to the blurring filters. The input to the registration method is taken from the blurring filters.

Figure 3: block diagram

Fixed and moving images are given to the image read and write filter. Depending upon the intensity of the pixel ratio image is been read or write. After the images are been read the output is given to the register filter. In this filter the two images i.e., fixed and moving images depending on the pixel intensities the two images get overlap and form a new image with both modalities in it. It is useful for the doctor to compare both the images of the same patient and check the results. Multimodality registration algorithm has the following steps.
1. **Feature detection**: Salient and distinctive objects (closed-boundary regions, edges, contours, line intersections, corners, etc) in both reference and sensed images are detected.

2. **Feature matching**: The correspondence between the features in the reference and sensed image established.

3. **Transform model estimation**: The type and parameters of the so-called mapping functions, aligning the sensed image with the reference image, are estimated.

4. **Image resampling and transformation**: The sensed image is transformed by means of the mapping functions.

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**Fig 4**: steps of multimodality algorithm

Boundaries or surfaces, in medical images are many times more distinct than landmarks and hence can be used for segmentation by locating high contrast surfaces. Surface matching algorithms are normally used for rigid body registration. The representation of surface methods is a surface-based approach for registering multimodality brain image. They fit a set of points extracted from contours in one image to a surface model and extracted from contours in the other image. The image that covers the larger volume of the patient, or the image that has a higher resolution if volume coverage is comparable, is used to generate the surface model. Another version of surface matching is to provide user with an interactive transformation package that allows the user to translate and rotate one image with respect to the other.

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**III. RESULTS & DISCUSSION**

In this paper we have presented and analyzed a method for registering multimodality medical images. The algorithm has given successful and reliable registration without relying on the limits. Followed by image registration in the medical applications, segmentation is needed to determine areas of interest in the image and in many cases accurate demarcation of objects yields valuable information. Quantification is often the ultimate goal especially in medical applications. We believe that it will be a useful document for researchers longing to implement alternative Image registration methods for specific applications.
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